



Computation of full-field displacements in a scaffold implant using Digital Volume Correlation and Finite Element Analysis

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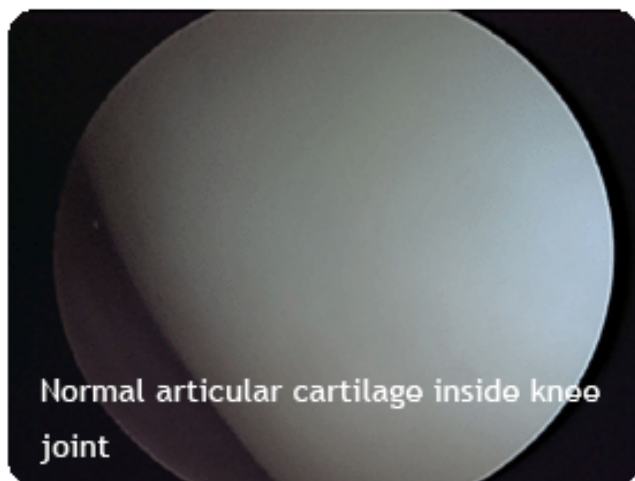
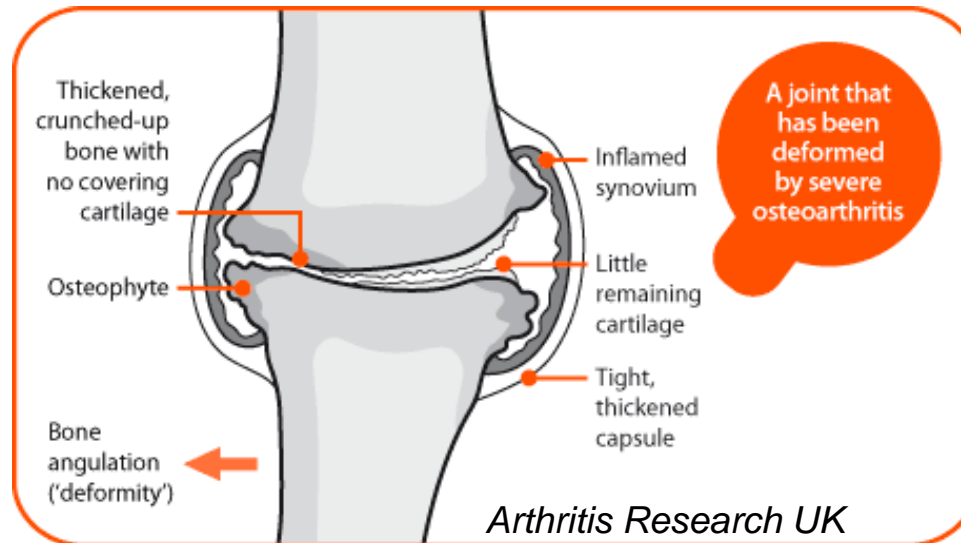
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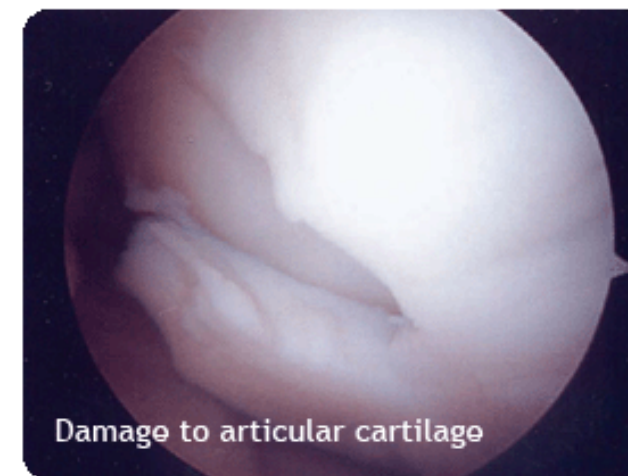




Osteoarthritis

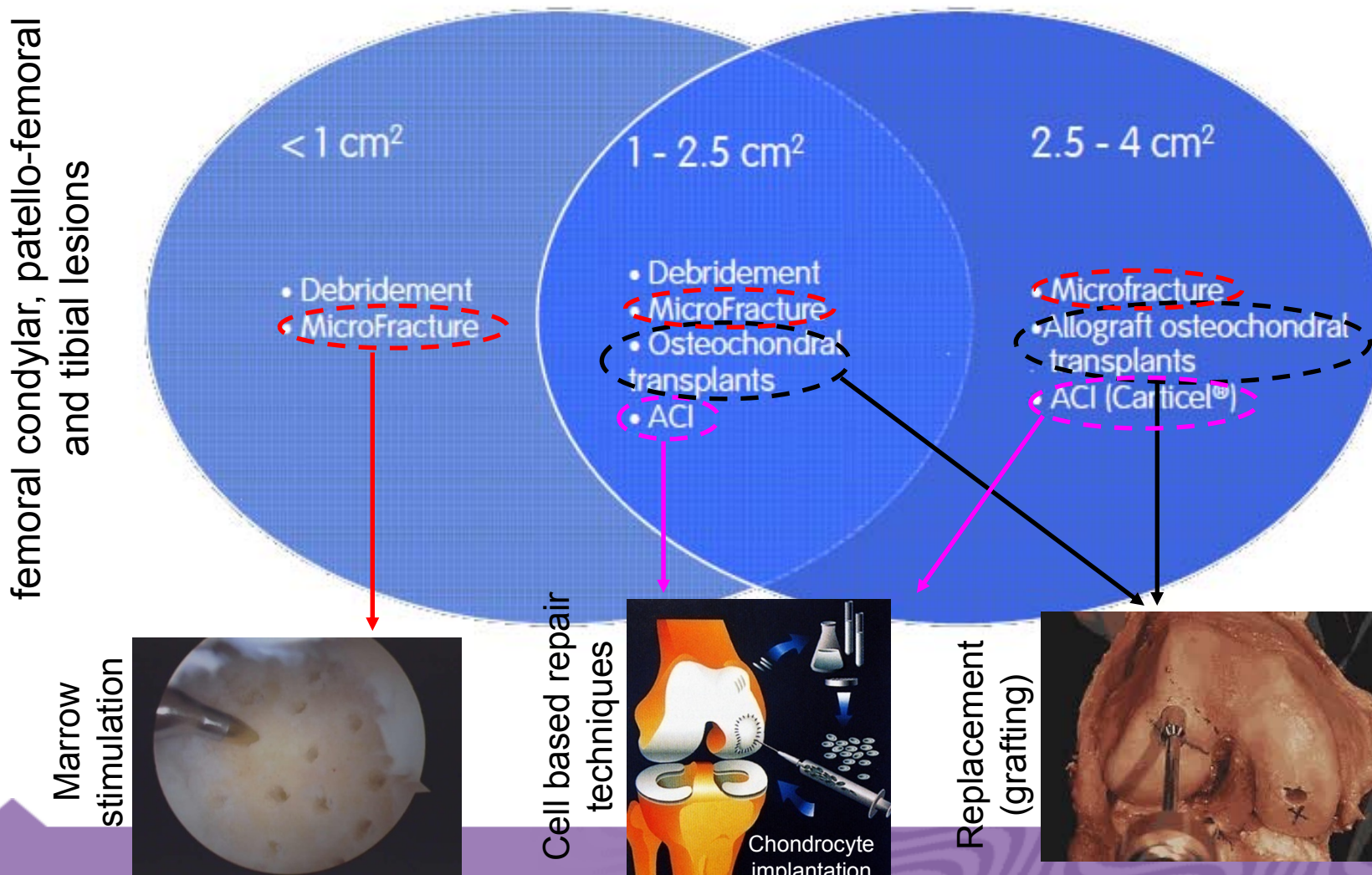


➤ Issue: cartilage has very limited capacity for self-repair !



Cartilage repair techniques

O.S. Schindler, *Articular cartilage surgery in the knee, Orthopaedics and Trauma 24:2*

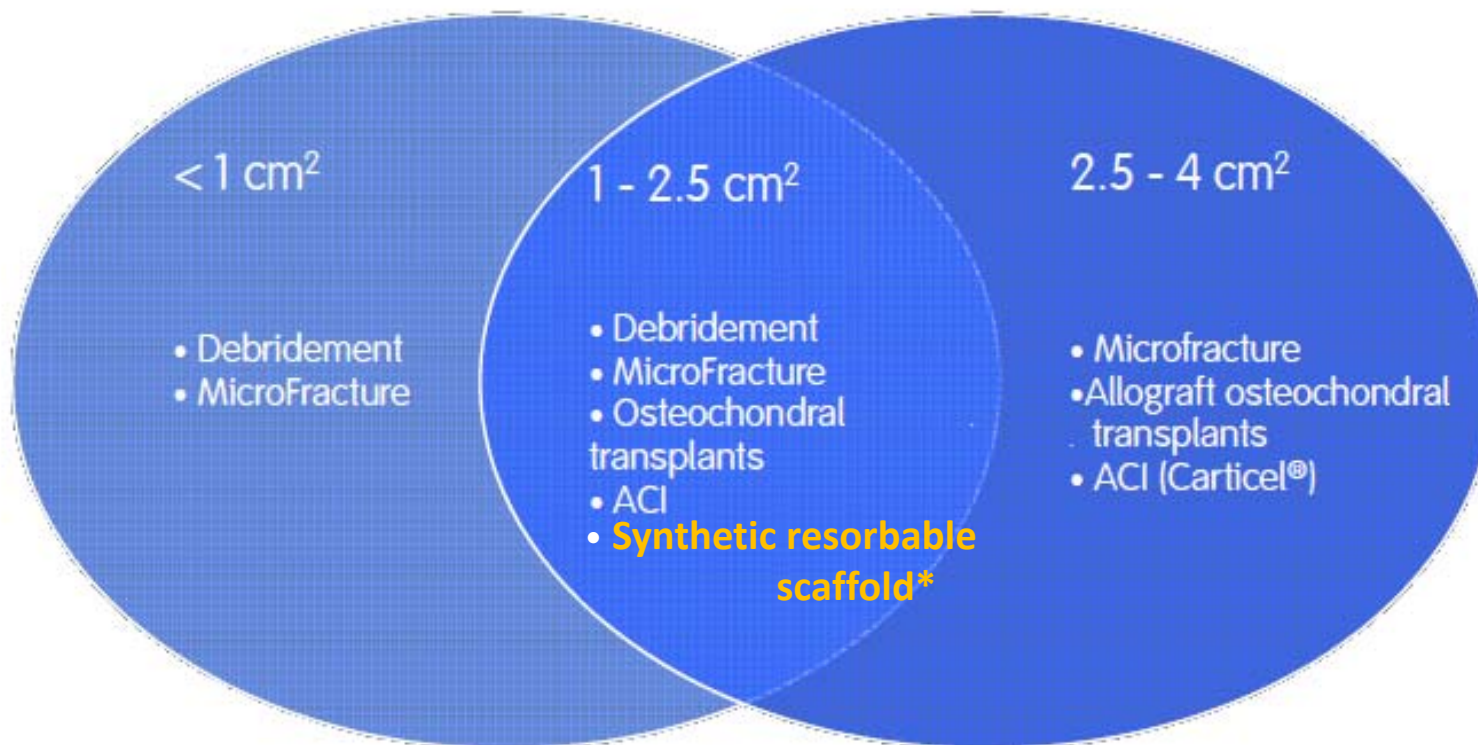




Engineering new cartilage using a biodegradable scaffold

O.S. Schindler, Articular cartilage surgery in the knee, Orthopaedics and Trauma 24:2

femoral condylar, patello-femoral
and tibial lesions



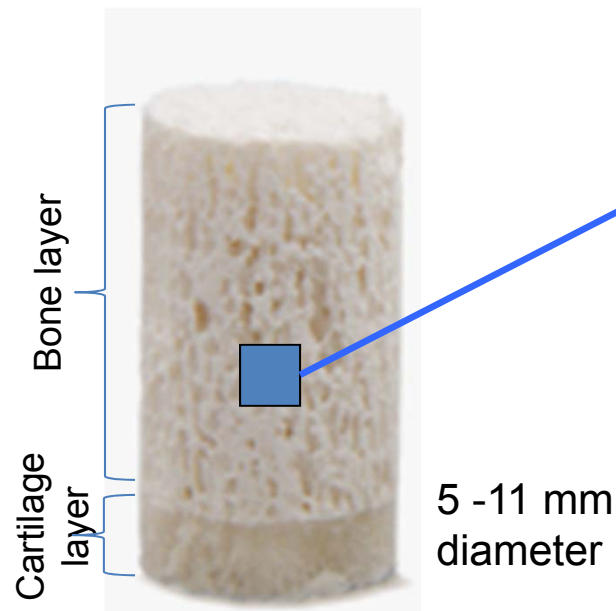
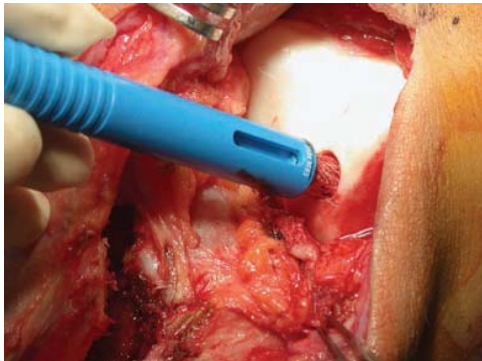
Trufit plug: biphasic scaffold

- Promising implant: Trufit plug scaffold (Smith & Nephew)
 - Designed to capture and retain bone marrow elements and encourage differentiation into articular cartilage and bone

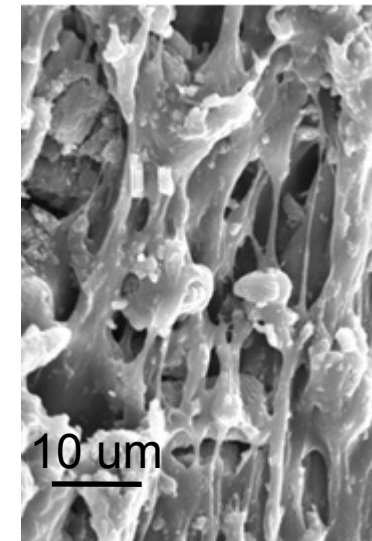
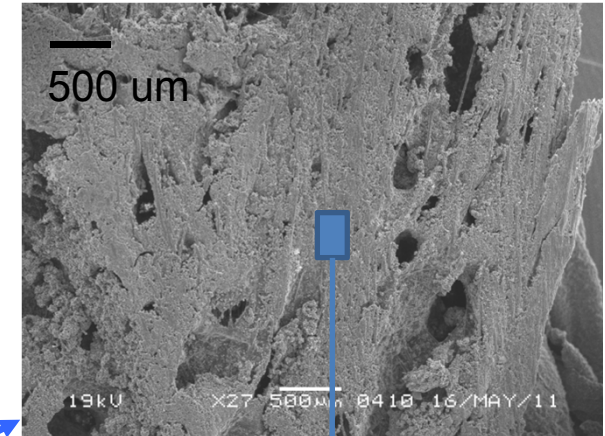
Creating a surgical
defect over the lesion



Implanting the plug



polylactide-co-glycolide (PLGA) matrix reinforced with polyglycolide (PGA) fibres, surfactant, and with calcium sulphate in the bone phase





Motivation

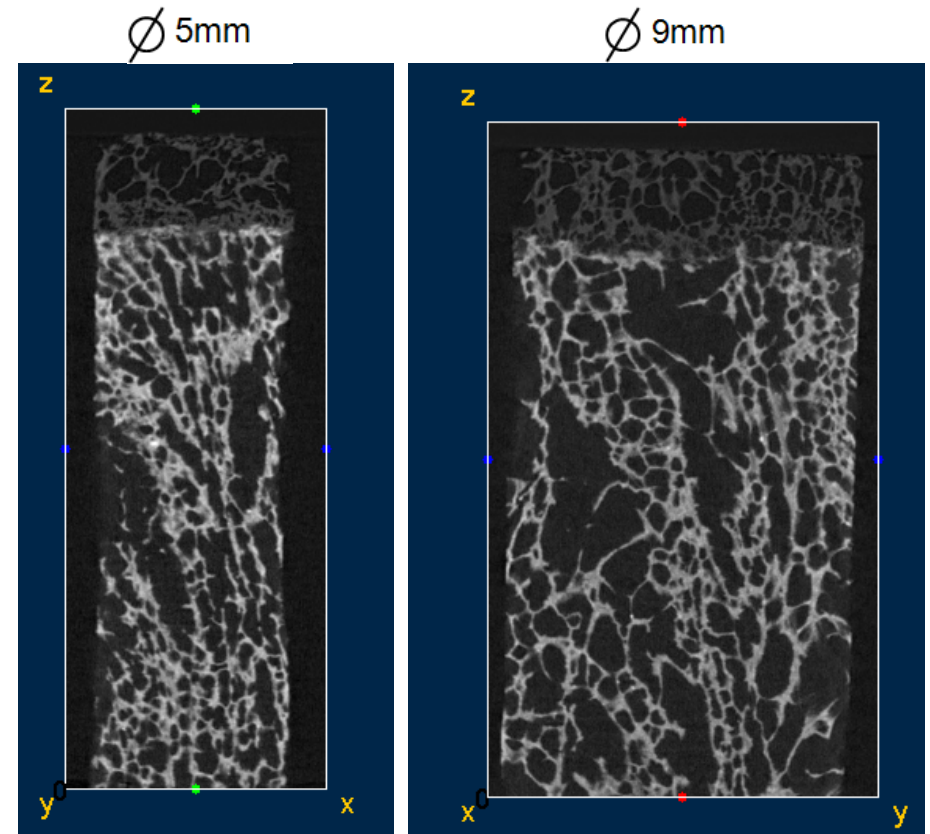
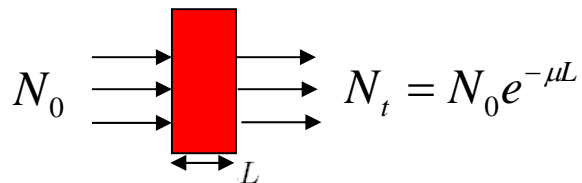
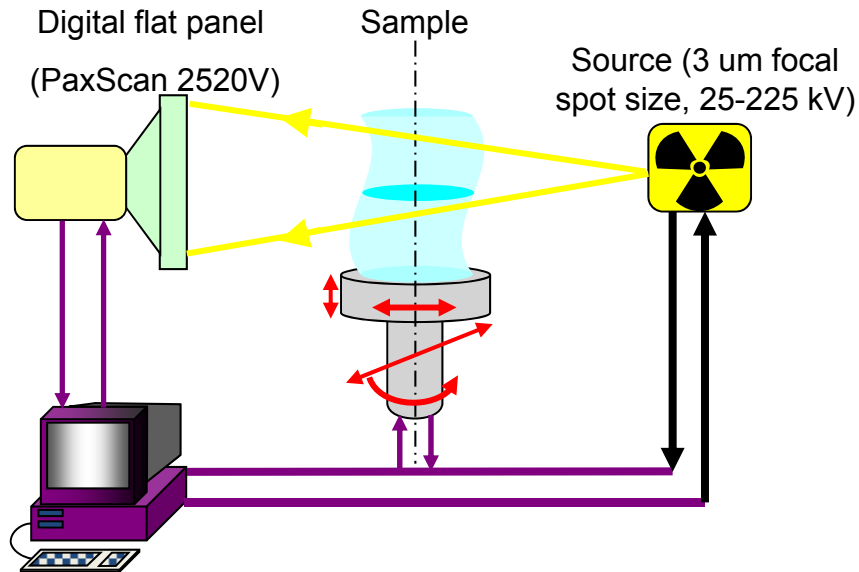
Although used in clinical procedures, little has been done to investigate the biomechanical behaviour of the implant under physiological conditions

In situ mechanical testing coupled with DVC is a valuable tool for characterizing the mechanical behaviour and for investigating the failure mechanisms

- Demonstrate the feasibility of the technique on the implant
- Assessment of the reliability of the DVC displacements and strain fields
- How DVC measurements compare with finite element predictions ?

3D representation of the morphology

CT scanner: Nikon Metris XT H 225

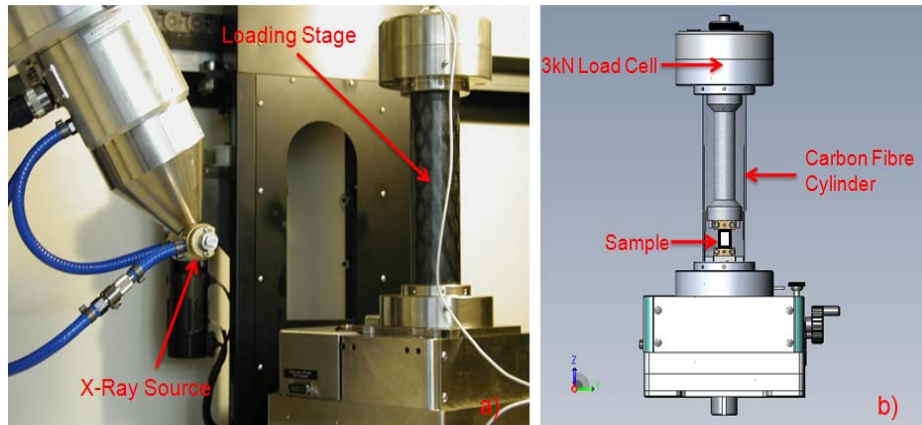


Voxel size: 20 microns
Energy = 51 kV / 160 μ A

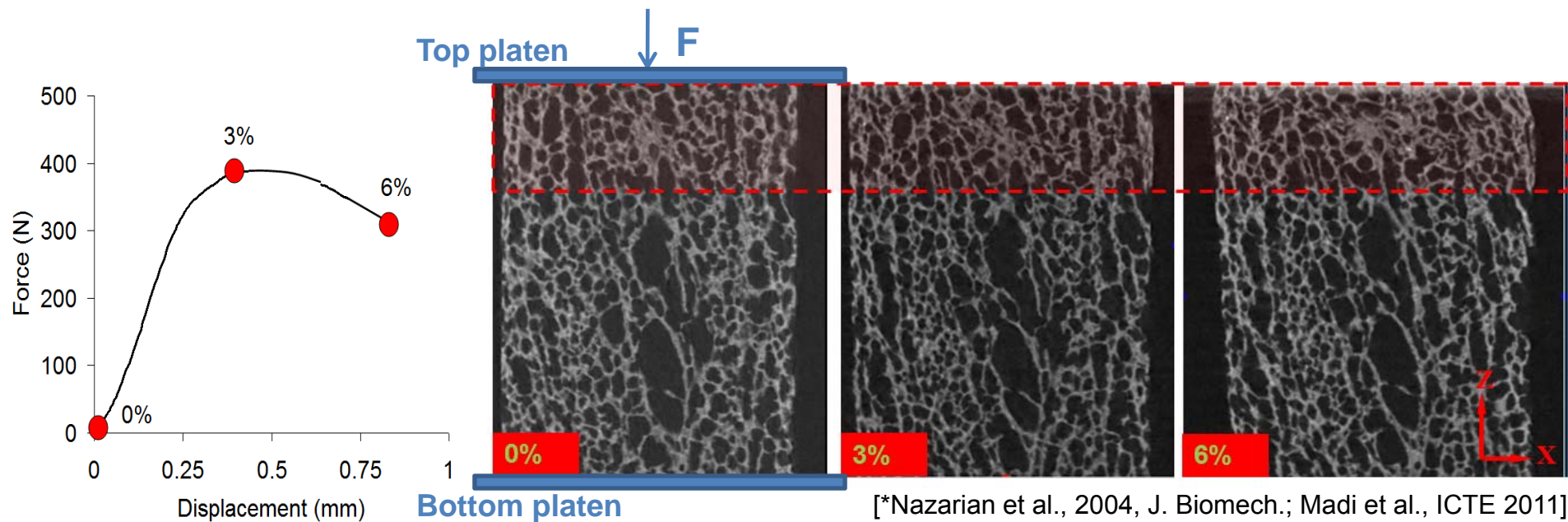
1500 angular projections, ~1 hour scanning time,
10 min reconstruction

In situ mechanical testing

Deben MICROTTEST



- Sample 14.7 mm length, 8.57 mm diameter, fixed on the lower compressive platen
- 15 min-window before CT acquisition (relaxation*)



[*Nazarian et al., 2004, J. Biomech.; Madi et al., ICTE 2011]

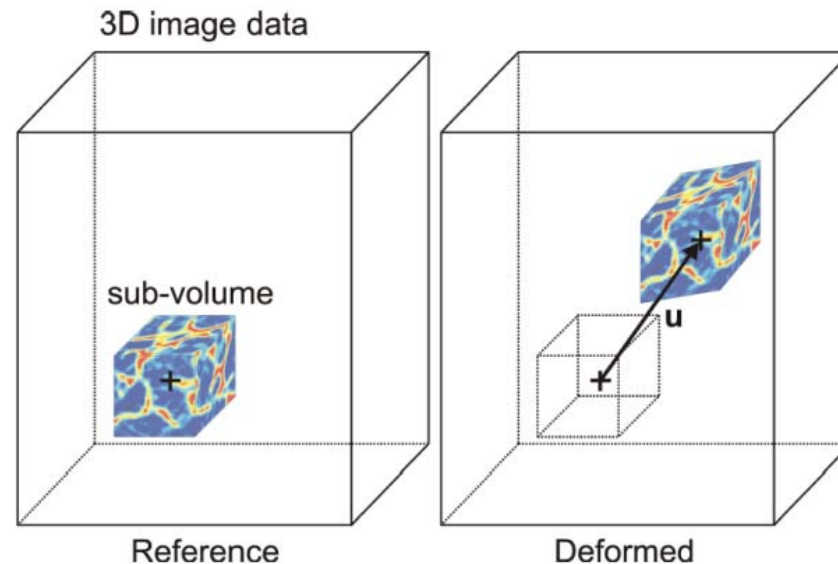


Digital Volume Correlation - Micro-FE modelling

- Two approaches of DVC have been mainly used: local approach and global approach.
- Systematic comparison of their performances and strain distributions is rarely reported, especially for biological tissues with foam-like morphologies [Liu et al., 2007, J. Biomech.]
- Micro-FE models have proven to be very powerful to understand and predict the mechanical behaviour of cellular materials [Muller et al., 1995, Med. Eng. Phys.; Youssef et al., 2005, Acta Mat.]
- First attempt to compare DVC measurements of cellular materials with FE predictions: [ZaueI et al., 2006, J. Biomech. Eng]. Good agreement along the loading direction but less accuracy along the lateral directions.

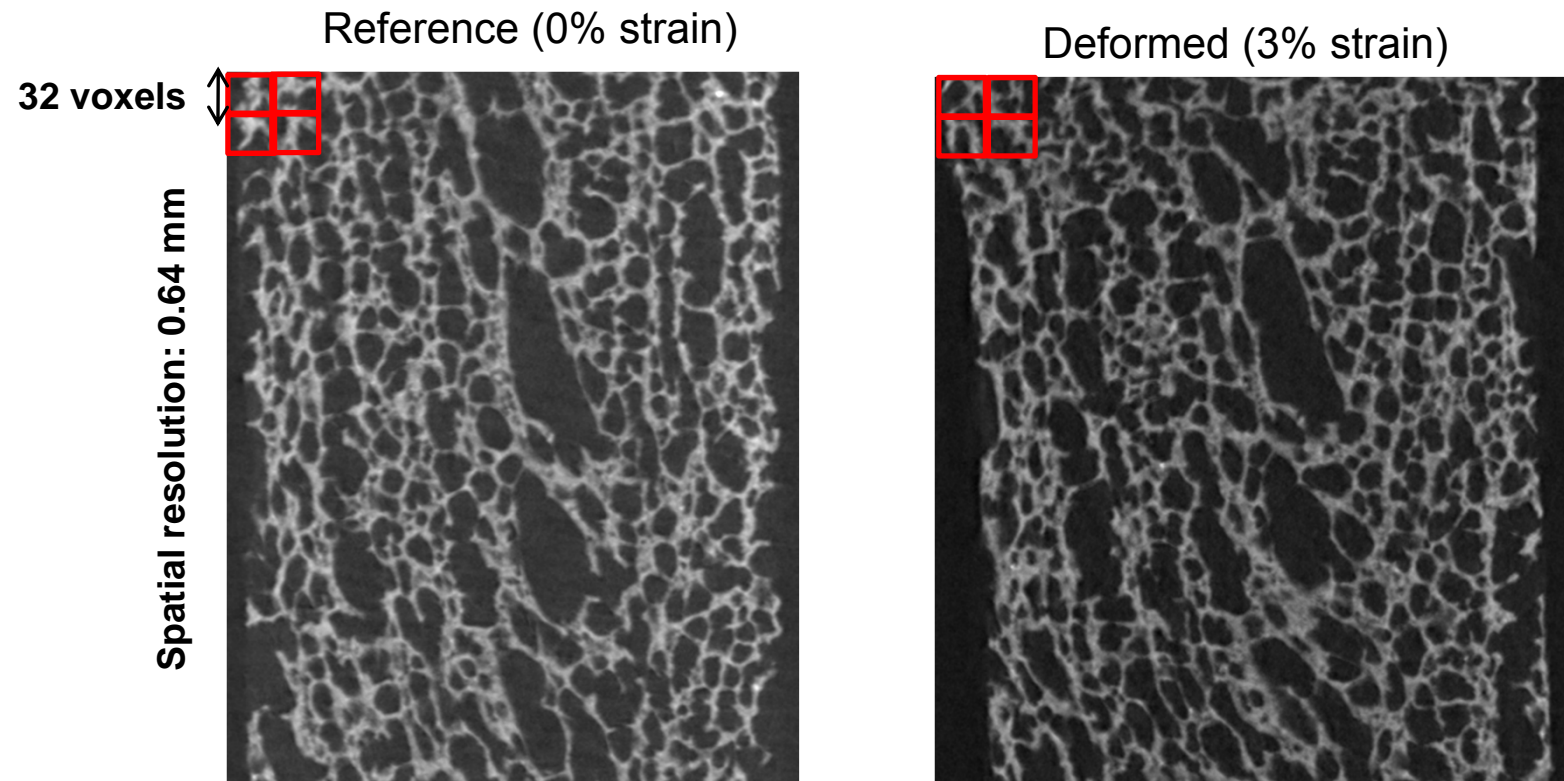
Local approach to DVC

- Gray level (2D or 3D) images $f(\underline{x})$, $g(\underline{x})$
- Principle of optical flow conservation: $f(\underline{x}) \cong g(\underline{x} + \underline{u}(\underline{x}))$
- Find the best match between grey level intensity of the reference and deformed image, in small zones of interest (cross-correlation, sum of squared differences)



*[Peters et al., 1982, Optics Eng.; Bay et al., 1999, Exp Mechanics; Bornert et al., Inst. Mes. Métrol, 2004; Verlhup et al., 2004, J. Biomech.; Quinta Da Fonseca, 2005, J. Microscopy.; Benoit et al., J. Biomech., 2009]

Local approach to DVC (LA-DVC)



- FFT algorithm (cross-correlation) implemented in DaVis* (LaVision, StrainMaster)
- Multi-pass approach
- Final sub-volumes: $32 \times 32 \times 32$ voxels³ overlapped by 75%

*[Quinta Da Fonseca, 2005, J. Microscopy; McDonald et al., 2011, Phys. Status Solidi B]

Global approach to DVC

- Principle of optical flow conservation: $f(\underline{x}) \cong g(\underline{x} + \underline{u}(\underline{x}))$
- Select a specific displacement basis $\underline{\varphi}_i(\underline{x})$
such that $\underline{u}(\underline{x}) = \sum_i a_i \underline{\varphi}_i(\underline{x})$
- Minimize correlation residuals*

$$\Phi^2 \{a_i\} = \iiint \left[f(\underline{x}) - \underbrace{g(\underline{x} + a_i \underline{\varphi}_i(\underline{x}))}_{\text{Linearization}} \right]^2 d\underline{x}$$



Finite element DVC (GA-DVC)

$$\begin{aligned}\Phi_{\text{lin}}^2(\delta \underline{u}) &= \int_{\Omega} [f(\underline{x}) - \hat{g}(\underline{x}) - (\delta \underline{u} \cdot \nabla f)(\underline{x})]^2 d\underline{x} \\ &= \sum_e \int_{\Omega_e} [f(\underline{x}) - \hat{g}(\underline{x}) - \delta a_i^e (\underline{\varphi}_i \cdot \nabla f)(\underline{x})]^2 d\underline{x}\end{aligned}$$

Elementary matrix and vector (e.g., C8P1*), Correli

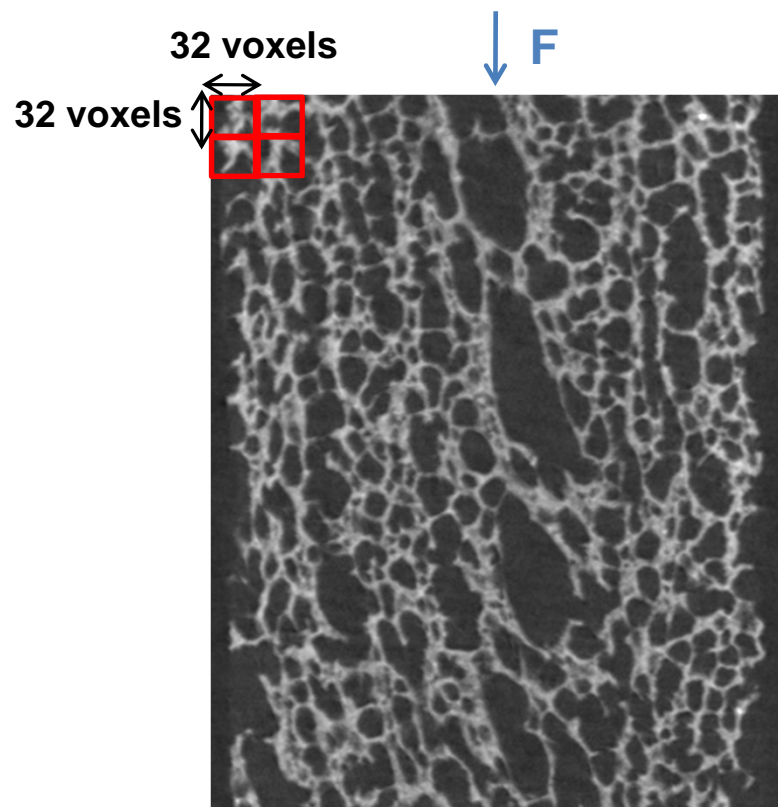
$$M_{ij} \delta a_j = b_i$$

$$\left| \begin{aligned} M_{ij}^e &= \int_{\Omega_e} (\nabla f \cdot \underline{\varphi}_i)(\underline{x}) (\nabla f \cdot \underline{\varphi}_j)(\underline{x}) d\underline{x} \\ b_i^e &= \int_{\Omega_e} [f(\underline{x}) - g(\underline{x})] (\nabla f \cdot \underline{\varphi}_i)(\underline{x}) d\underline{x} \end{aligned} \right.$$

- Multi-scale approach to deal with secondary minima and to be consistent with Taylor approximation*

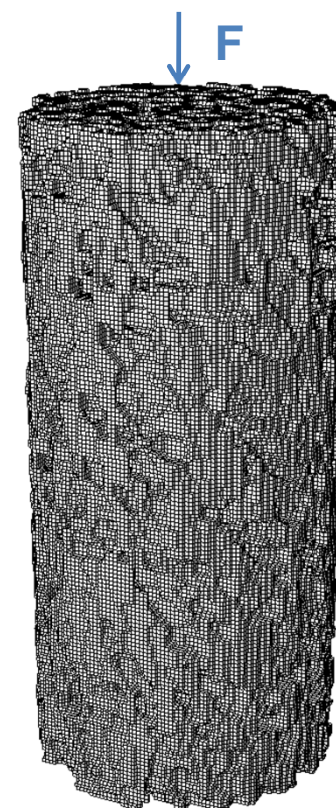


DVC vs FE comparison



DVC method: continuum level

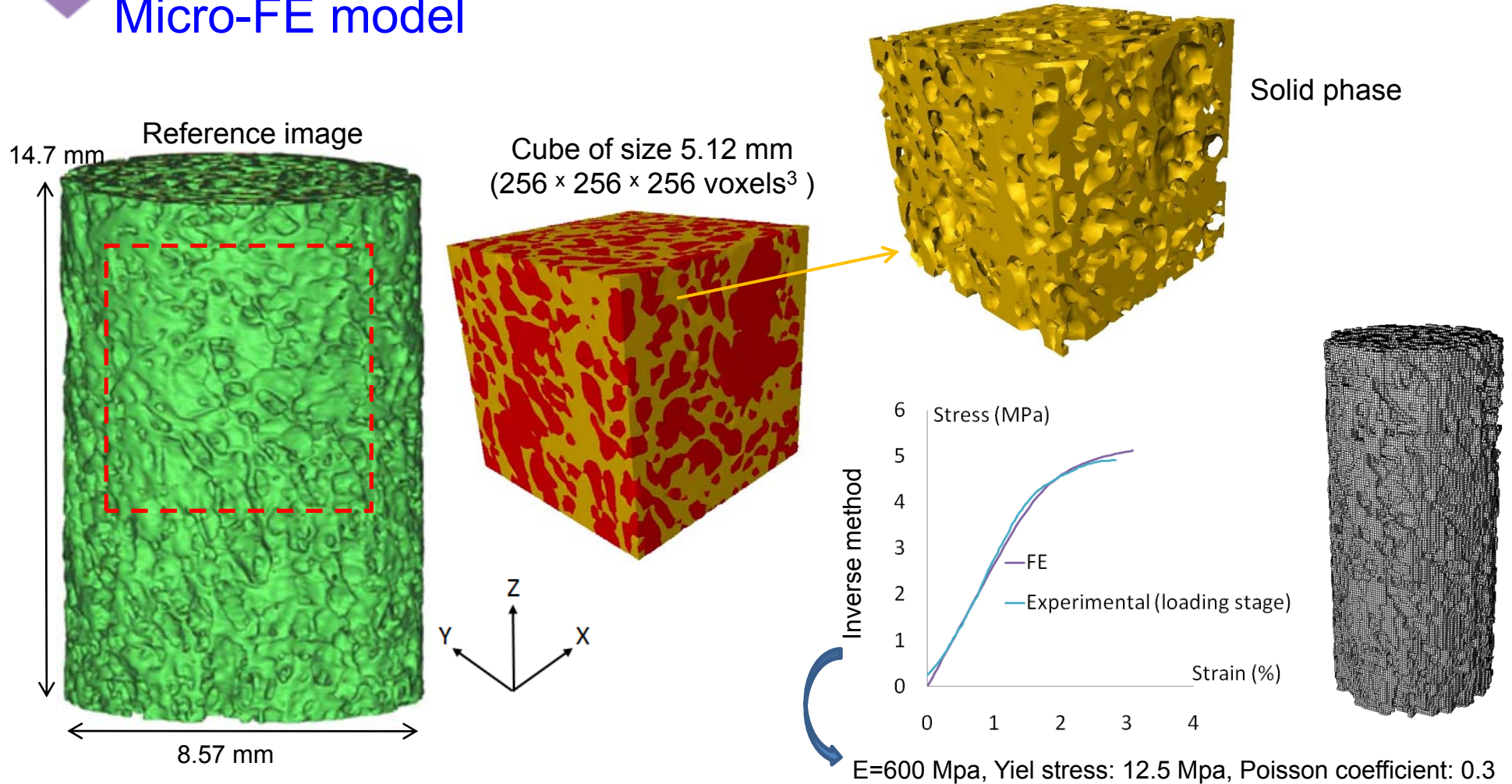
?



FE method: strut level

- Size of the sub-volumes: 0.64 mm > size of the pore walls (struts~0.1mm)

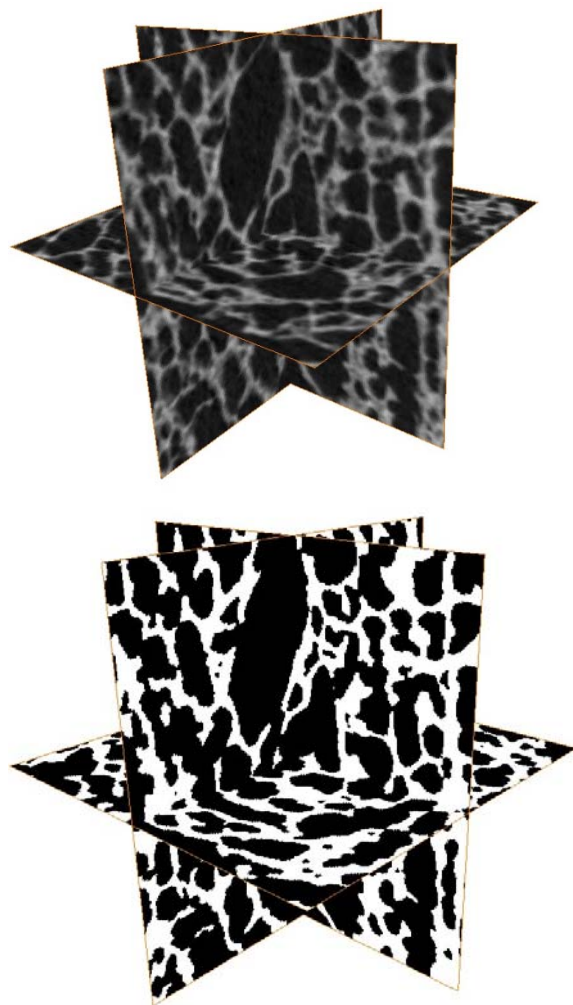
Micro-FE model



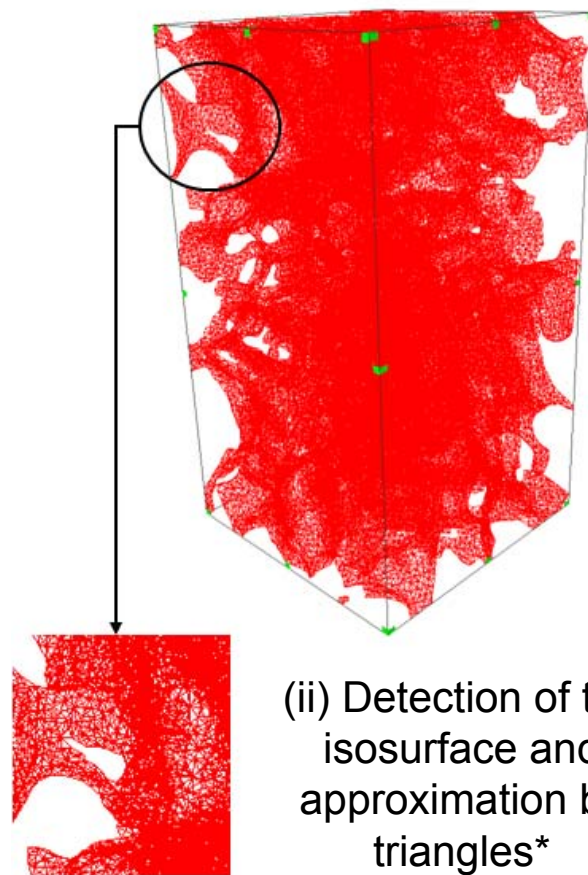
- Solid phase: elastic perfectly plastic
- Porous phase: linear elastic (contrast: 10000)



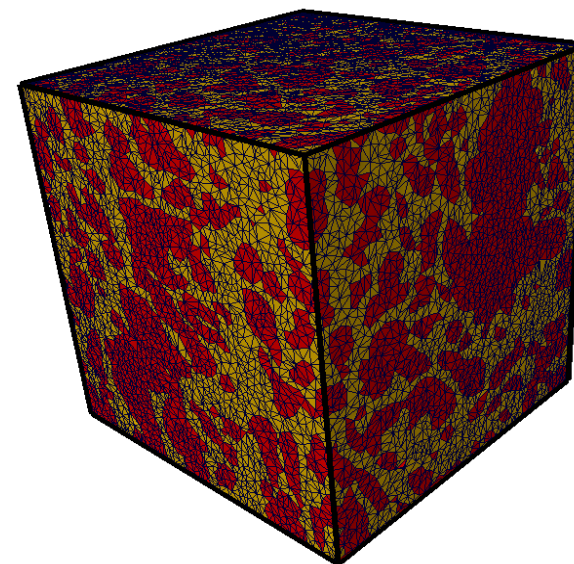
3D meshing



(i) Binarisation



(ii) Detection of the
isosurface and
approximation by
triangles*

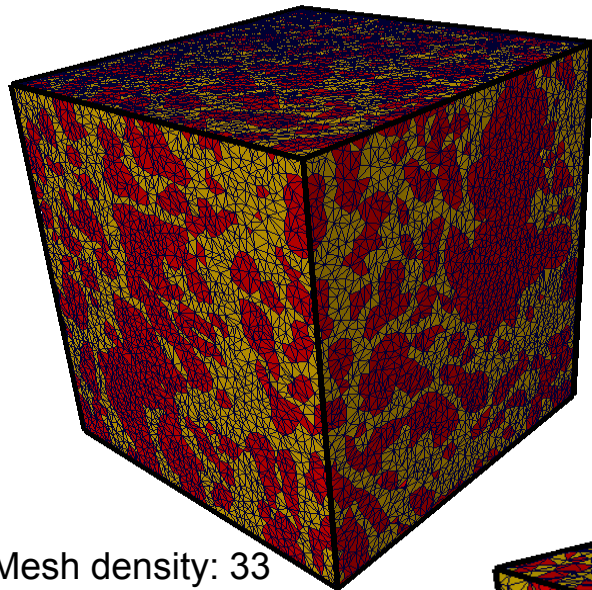


(iii) Volumetric grid*
(tetrahedra)

Mesh density: 33
voxels/element

*[Avizo, <http://www.vsg3d.com/avizo/standard>]

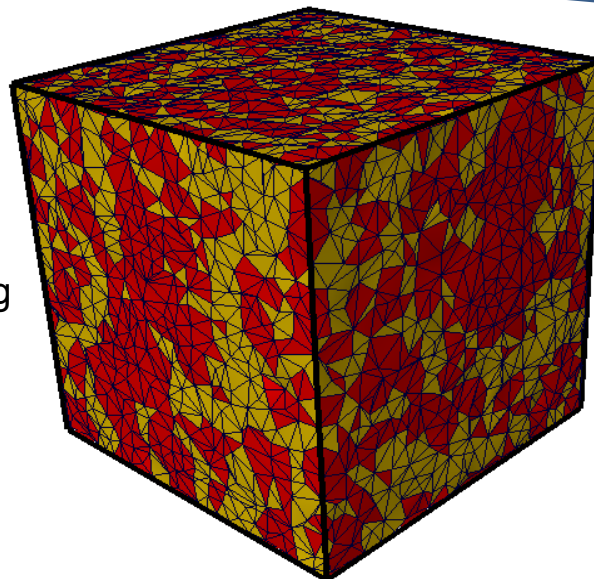
Boundary conditions



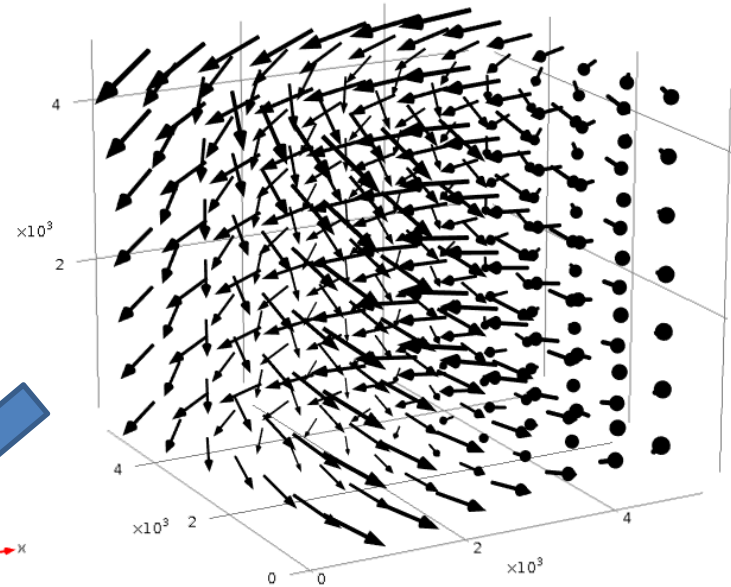
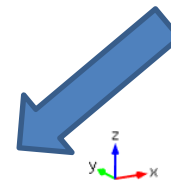
Mesh density: 33
voxels/element



Edge collapsing
algorithm*



Mesh density: 795
voxels/element (LA-DVC:
512 voxels/sub-volume)



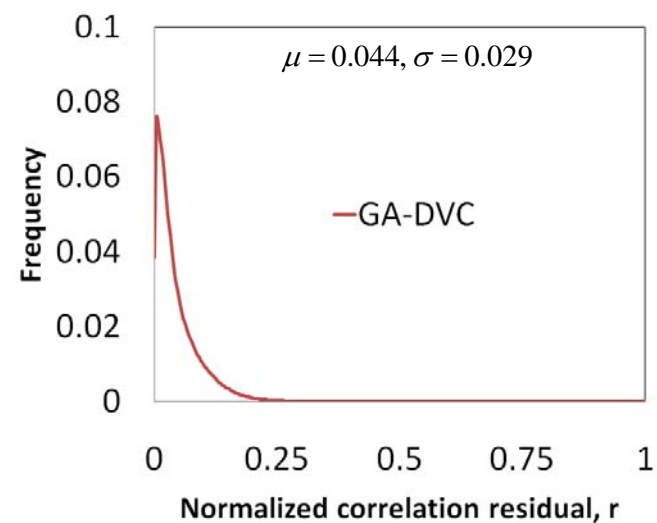
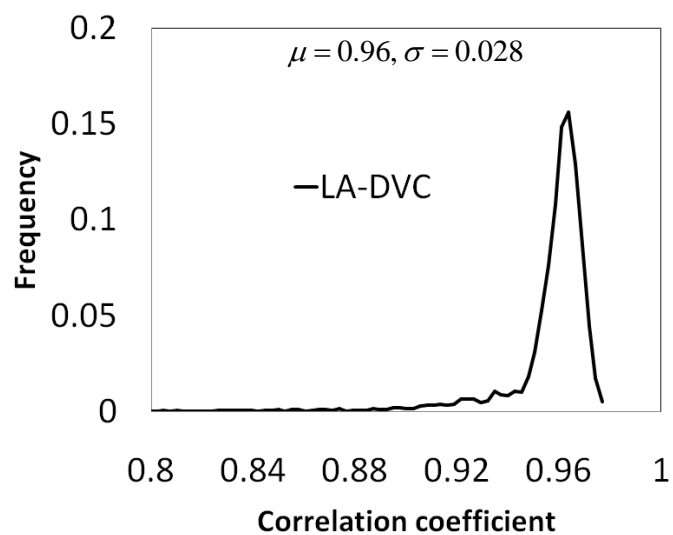
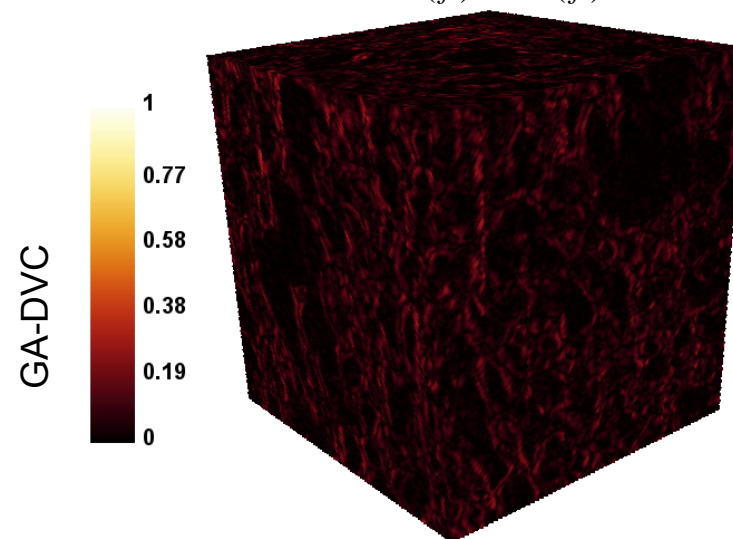
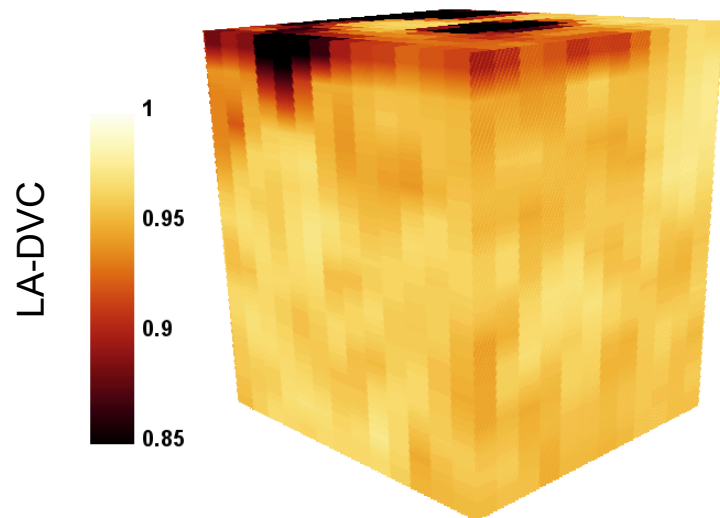
Displacement vectors obtained by
DVC applied as boundary conditions
at the mesh faces

*[Avizo, <http://www.vsg3d.com/avizo/standard>]

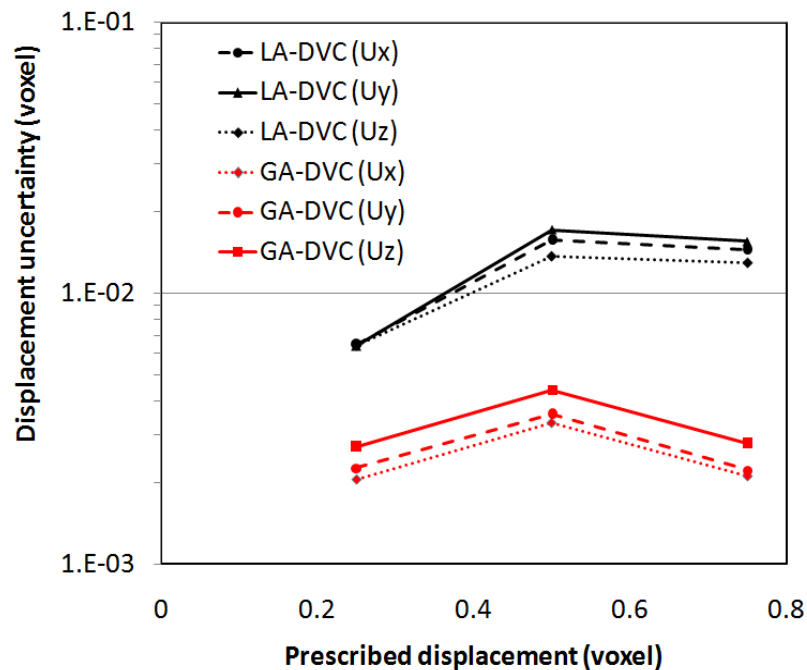


Correlation quality

$$r = \frac{\langle |g(x) - f(x + u(x))| \rangle}{\max(f) - \min(f)}$$



DVC Accuracy (subset size: 32 voxels)



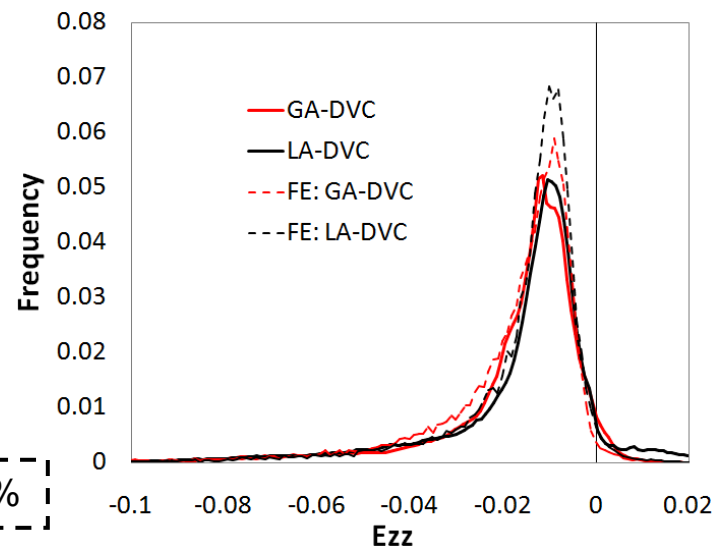
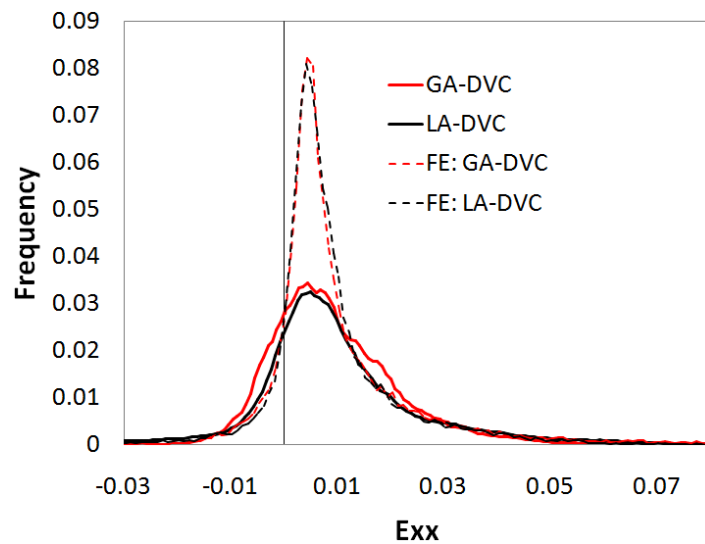
Prescribed displacement (voxel)	DVC method	Spatial average displacement (voxel)		
		$\langle u_x \rangle$	$\langle u_y \rangle$	$\langle u_z \rangle$
0.25	GA-DVC	0.249955	0.249997	0.249941
	LA-DVC	0.244904	0.245639	0.244712
0.5	GA-DVC	0.500000	0.500094	0.500024
	LA-DVC	0.490688	0.494992	0.490341
0.75	GA-DVC	0.750023	0.750081	0.750073
	LA-DVC	0.741899	0.738276	0.737006

GA-DVC: Global approach to DVC; LA-DVC: Local approach to DVC

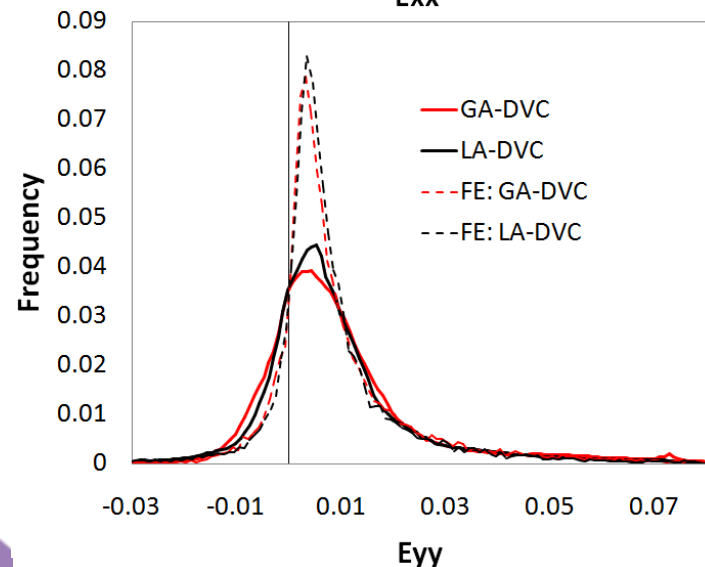
➤ Displacement uncertainty:

- Local approach: 0.006-0.02 voxel
- Global approach: 0.002-0.004 voxel

Strain distributions (subset size: 32 voxels)



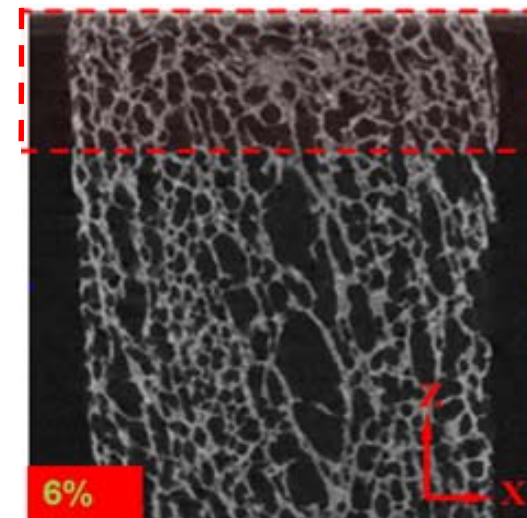
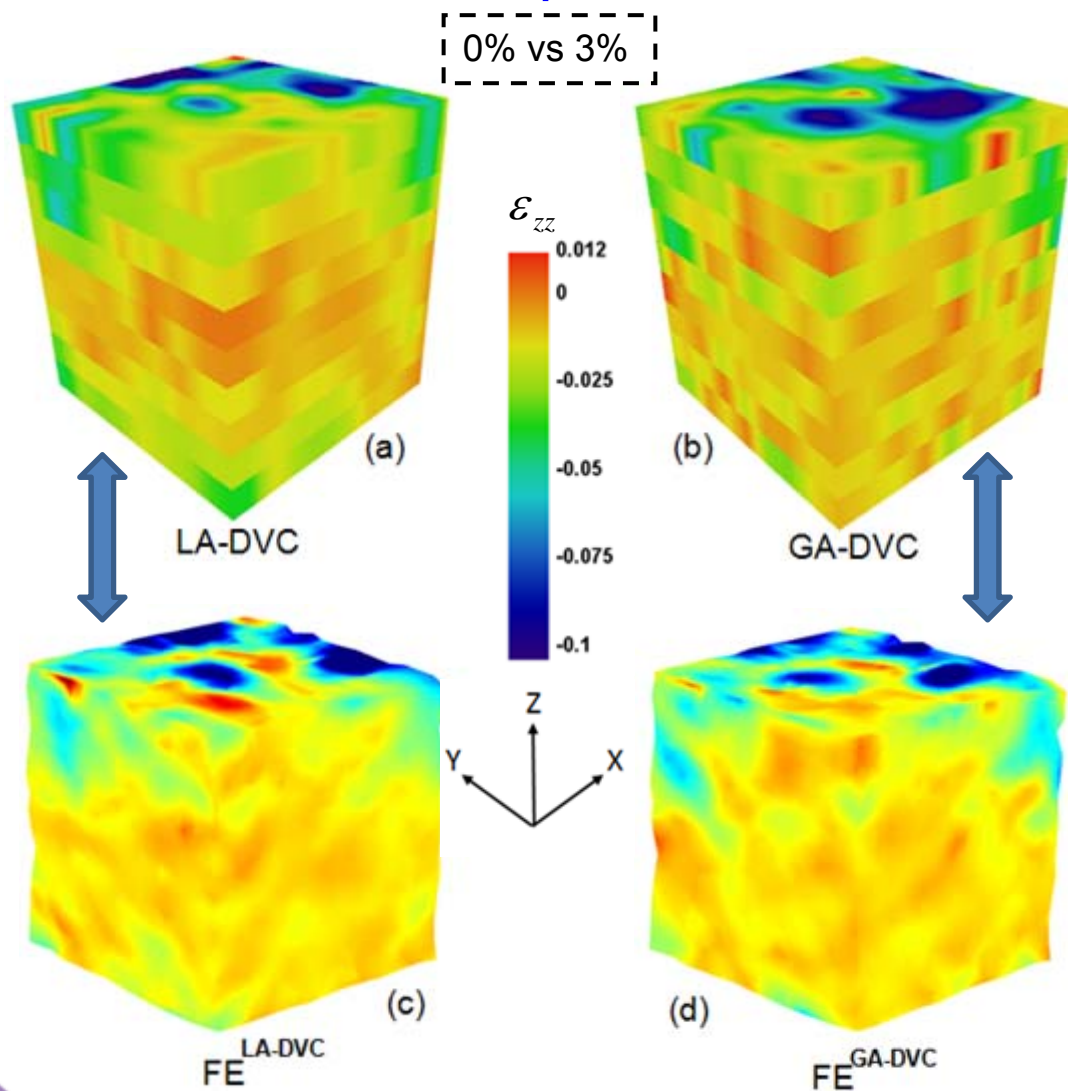
0% vs 3%



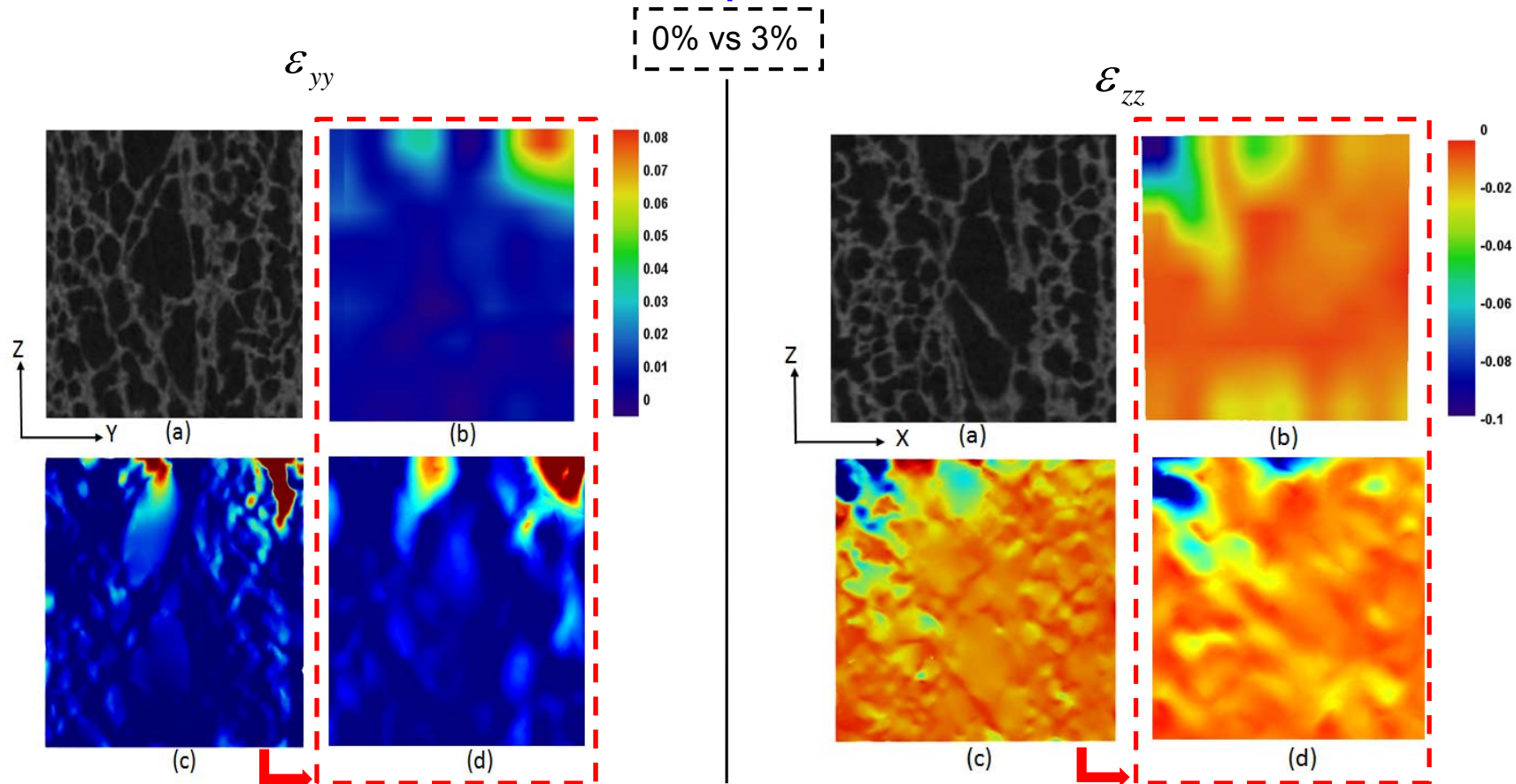
	$\langle E_{xx} \rangle$	$\langle E_{yy} \rangle$	$\langle E_{zz} \rangle$
Method	Std(E_{xx})	Std(E_{yy})	Std(E_{zz})
LA-DVC	0.0094	0.0097	-0.0176
GA-DVC	0.0095	0.0105	-0.0172
FE _{LA-DVC} model	0.0144	0.0170	0.0184
FE _{GA-DVC} model	0.0094	0.0105	-0.0173



Vertical strain map



Lateral and vertical strain maps



- (a): 2D section extracted at the core of the VOI
- (b) DVC: 512 voxels/subvolume
- (c) FE: 33 voxels/element
- (d) FE: 795 voxels/element

Discussion (1)

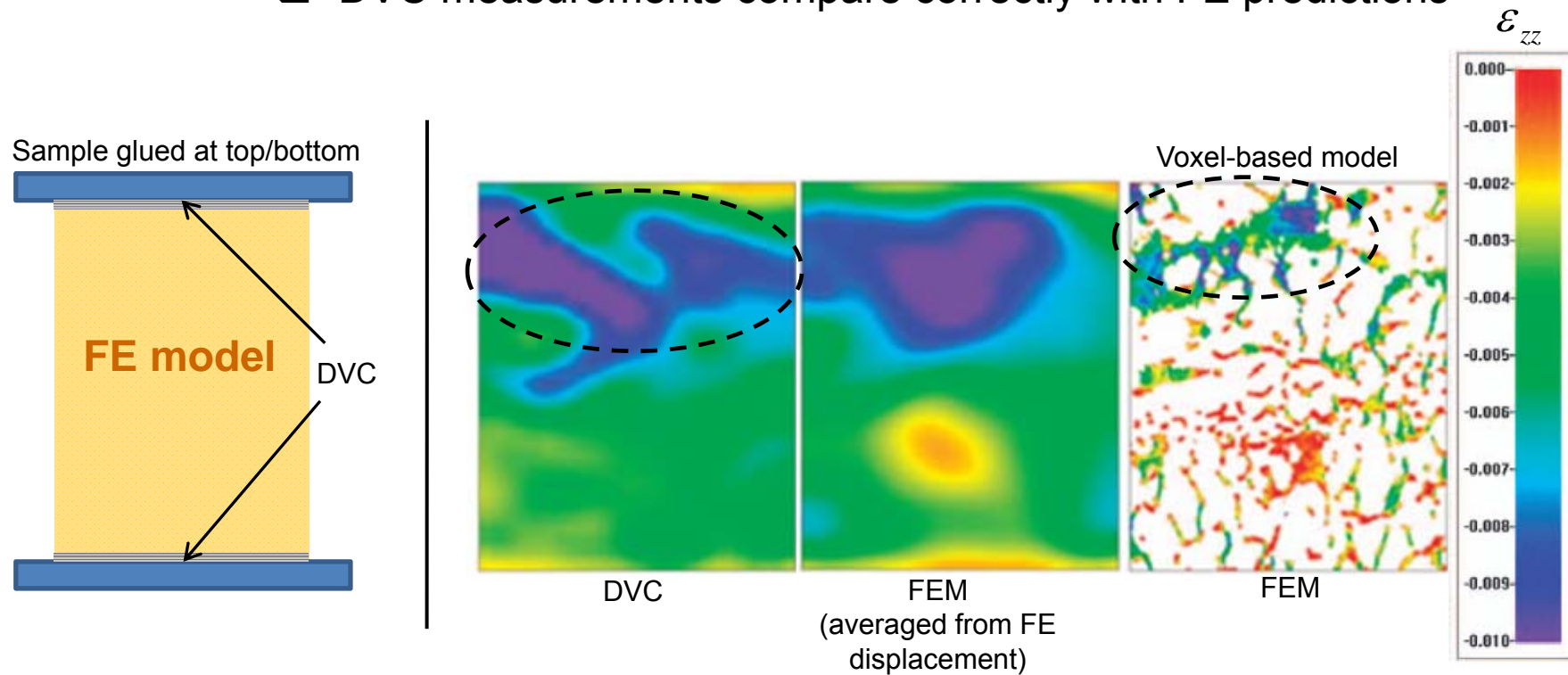
- ❑ Strains maps and histograms obtained with the local approach are in good agreement with those obtained with the global approach

- Local approach:
 - FFT combined with the multi-pass approach allowed fast calculations with displacement uncertainties ranging from 0.006 to 0.02 voxel
 - Literature*: 0.005 – 0.056 voxel

- Global approach:
 - Displacement uncertainty can be reduced by a factor ranging from 3 to 10.
 - Might be suitable for applications where small strain levels are required ?

Discussion (2)

- DVC measurements compare correctly with FE predictions



Previous work*:

- vertical strain: good agreement
- lateral strains: smaller predicted strains than measured

*[ZaueI et al., 2006, J. Biomech. Eng.]



Conclusions

- In situ uniaxial compression combined with DVC performed on a scaffold implant developed for knee repair purposes
- Displacements and strains assessed using two different approaches to DVC
- Strain measurements compare well with FE predictions
- Feasibility of the DVC technique demonstrated

Perspectives

- Comparison of mechanical behaviour and failure mechanisms of the implant with that of native tissues: trabecular bone, cartilage